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Experimental Design Analysis of 3D Printing Processes in the Optimization of Material Mechanical Properties

Shaobiao Cai, Minnesota State University; Sairam Vangapally, Minnesota State University; Yongli Zhao, St. Cloud State University

Abstract

Mechanical properties, such as strength of materials, are among the most important material properties in engineering, supporting applications such as mechanical systems and artificial bones in biomedical applications. With the application of additive manufacturing, such as 3D printing, complex structures can be achieved efficiently, greatly broadening engineering design and fabrication capabilities. However, the mechanical properties of the 3D-printed part of a system need to be optimized. In this paper, the authors present insights into the effects of design structures and additive manufacturing factors to the strength of commonly used PLA and stainless steel 316. Experimental design techniques were used to study parameters such as building temperature and layer thickness. The optimum factors of parameters for achieving better strength of the PLA and stainless steel are identified. The design structures of stainless to the strength property of the parts were compared and analyzed. Recommendations for achieving better strength using additive manufacturing are also made.

Introduction

Additive manufacturing (AM) is a method for creating a product through layers. Typical examples include fused deposition, binder jetting, selective laser sintering, material jetting, and selective laser melting. These methods can handle almost any material, including polymer, metals/metal alloys, ceramics, and composites. According to Torres, Sandback, and Cai (2018):

AM allows parts to be designed with extremely complex geometries and at low cost compared to other manufacturing processes. AM also offers the ability to fabricate different parts using the same machine, making it appealing for low volume product production which would otherwise be prohibitively expensive. (p. 26)

Although AM is capable in handling myriad materials and features, limitations do exist. One of the major concerns is the strength of the final part or system built. This is related to the mechanisms of the way that the material is fused or bonded. A typical example is the effect of temperature on the property of the built part. The final part may be very weak if temperature is not appropriately controlled. This may make the part useless. To broaden the practical applica-

tions of AM, further study on the fabrication factors that affect the properties of the materials is needed. As stated in earlier studies, as additive manufacturing becomes more prevalent, it is necessary to understand how the mechanical properties of the final products can be controlled (Torres et al., 2018; Kobryn, Moore, & Semiatin, 2000; Es-Said, Foyos, Noorani, Mendelson, & Marloth, 2000; Ahn, Montero, Odell, Roundy, & Wright, 2002).

For additive manufacturing, the properties largely depend on the building method and the specific technology used. For instance, fused bonding with powder material and filament can be different. Fusion of adjacent layers typically dominates the properties of material. Filament and deposition orientation largely determine the anisotropic properties of the material. Many build parameters an affect the material properties of the final product. These parameters include the number of contours within a layer, building orientation, raster angle, air gap, deposition speed, volume rate, temperature, etc. Material property change with AM build parameters, such as build orientation, raster angle and nozzle diameter has been reported (Torres et al., 2018).

Numerous researchers have conducted studies on 3D printing technologies and related factors (Bellini & Güçeri, 2003; Lee, Abdullah, & Kahn, 2005; Lee, Kim, Kim, & Ahn, 2007; Sood, Ohdar, & Mahapatra, 2012). Bellini and Güçeri used fused deposition modeling to study the mechanical characterization of fabricated products. Lee et al. (2005) studied the properties of the product prototype by changing factors such as filament size, building path, and intervals. In addition, the material compressive strength was investigated by Lee et al. (2007) and Sood et al. (2012). Lee et al. (2007) further examined the strength in various directions (anisotropic properties), while Sood, Ohdar, and Mahapatra (2010) studied various factors such as raster angle, orientation, thickness of layers, etc. Different building materials such as thermoplastic ULTEM 9085 (Bagsik, 2011), bioextruded poly (Domingos, Chiellini, Gloria, Ambrosio, Bartolo, & Chiellini, 2012), ABS (Ziemian, Sharma, & Ziemian, 2012), lattice material (Park, Rosen, Choi, & Duty, 2014), Ti-6Al-4V (Carroll, Palmer, & Beese, 2015), periodic lattice structure with selective laser melting AM method (Liang, Raymont, Yan, Hussein, & Young, 2011), foam/porous material (Gabbrielli, 2009), and porous metal structure (Furumoto, 2015) were studied using this technology as well. All of these studies presented valuable knowledge about the various factors for a specific AM technique. Torres et al. (2018) explain that among the building

parameters, some of these parameters may play more significant roles than the others in affecting the material properties of the final product; and, it is expected that the individual parameters with the greatest effect can be obtained.

In this current study, the authors performed a comprehensive study of previous work as well as current work demonstrating that the different effects of the various factors involved and further showing that these factors can be optimized. As a comparison, both the fused deposition technique for polylactic acid (PLA) and binder jetting for stainless steel 316 are presented. Fused deposition uses extruding the molten material (melts) on a defined path; each previously built layer cools readily and forms the foundation for a new layer. Binder jet additive manufacturing, however, uses a binding agent to join the powder particles. Furthermore, each type of printer differs. Even within the same type, individual printers can be different. This current study used a well-established experimental design method aimed at providing reliable, tested direction/guidelines for obtaining preferable material properties when using additive manufacturing technology.

Design Experimentation

The design experimentation of PLA and stainless steel (SS316) are presented below. For this study, it was assumed that: the parameters were independent from other parameters not involved in the study and that the number of levels was sufficient; the machines could produce reliable samples; and, the Taguchi experimental design technique used could deliver reliable results. This method is widely used in industry and academic fields to investigate the effects of multiple factors and multiple levels of each factor experimentally. With this method, full arrays of combinations may be avoided when the combinations are huge, and partial fractions of a limited number of trials may be used to produce the most information. More details may be found in Torres et al. (2018).

Design with PLA

PLA has been studied recently (Torres et al., 2018). In this current study, three parameters—extruding temperature, deposition rate, and layer thickness—were used to investigate the factors affecting the properties of PLA, and three levels of each parameter were tested. Some of the data are presented here for comparison. These levels were defined as 1 (low level), 2 (medium level), and 3 (high level). The levels corresponding to each of the parameters were 200°C (1), 225°C (2), and 200°C (3) for extruding temperature (T); 30 mm/s (1), 55 mm/s (2), and 80 mm/s (3) for deposition rate (D); and 0.05 mm (1), 0.13 mm (2), and 0.20 mm (3) for layer thickness (L). For notation, the sample made under T1D1L1 indicates that the operation parameters were at a lower temperature (200°C), lower deposition rate (30 mm/s), and lower thickness (0.05 mm). For the tempera-

ture, the limits were not used in order to avoid potential unstable issues with the machine. Rather, the high limit used was 10°C below the maximum, and the low limit was 20°C higher than the minimum. As with the extruding temperature, levels for the other two parameters were within the capability of the machine as well for the same reason.

For the experiment design, the Taguchi method was used. Based on this method, a partial of nine experimental trials were defined. These nine trials were expected to convey the same information as a full array of 27 trials without losing significance for the three-parameter three-level studies. Three samples were created for each parameter level in the study. The details of the combination array were presented in Torres et al. (2018). Ultimaker machine was used to make the PLA sample bars, and the binder jetting-based ExOne M-lab machine was used to make the stainless steel 316 samples. The PLA samples were first designed with Creo. The computer models were then converted to an STL file and then inputted into the Ultimaker machine in order to create the sample bar using configurations mentioned earlier with the standard Taguchi partial combination array. Three sample bars were created for each trial, and a total of 27 samples were used to examine the effect of the selected parameters. The samples were tested using an MTS machine for tensile strength; details are presented in the Results and Discussions section. The MTS tester was calibrated by the professionals from the MTS Company under testing equipment standards.

Design with Stainless Steel 316

To study the mechanical strength of stainless steel 316 built with AM, binder jetting technology was used. This machine has the ability to build metal and metal alloy materials. Stainless steel 316 was chosen for this study, given the many applications of stainless steel. Table 1 shows the components of this alloy. Layer thickness, sintering time, and sintering temperature were the three parameters selected for the study, and each parameter could vary from low to high levels (two levels). For the three-parameter, two-level experimental design, a full factorial experimental approach was used. Table 2 lists the three process parameters at the corresponding two levels used to set up the machines.

Table 1. Chemical composition of SS316 (wt%).

C	Mn	P	S	Si	Cr
0.08	2.00	0.045	0.03	0.75	16.00-
max	max	max	max	max	18.00

The full factorial design of experiments, three parameters and two levels each, yielded a total of $2^3 = 8$ experimental combinations. Two samples were created for each parameter. Table 3 shows the design of the three parameters and two levels of the experiment. In the study, all eight possible combinations were tested. This experimental design was used to produce the parts for the study. The sample used in

the study was a solid cylinder, 25 mm in length and 10 mm in diameter. To create the samples, the CAD model was designed in Creo Parametric 3.0. Then the CAD model was sliced into layers and the STL model was inputted into the ExOne M-lab machine for printing. The 3D printing process started by loading the stainless steel 316 powder into the bed. Along with the powder, the STL file, binding agent, and cleaning agent were loaded. The powder had an average particle size of 30 µm; the material was obtained from Ex-One and used with no further treatment. Figure 1 shows the samples created with the ExOne M-lab machine. Various structures (with/without lattice) were fabricated so that the structural effect could be studied. However, the focus of this current study was on the solid cylindrical structure without lattice; research on the structural analysis will occur in future studies. Compression testing on the samples followed ASTM E9 standards for metallic materials. An MTS 810 material testing machine with a 1KN load cell at a constant crosshead speed of 0.1 in/min was used, and the data were recorded for every 0.05 seconds.

Table 2. Process parameters and levels.

Factor	Low Level (0)	High Level (1)
Layer thickness(A), µm	50	100
Sintering time(B), hours	2	4
Sintering temperature(C), °C	1120	1180
Material: SS 316	•	

Design: Cylindrical solid with 25mm length, 10mm diameter

Machine: ExOne X1 lab 3D printer

Table 3. Full factorial experimental plan with low-level (0) and high level (1): A (low 50μm, high 100 μm); B (low 2 hours, high 4 hours); C (low 1120° C, high 1180° C).

Experiment	Layer Thickness(A)	Sintering Time(B)	Sintering Temperature (°C)
1	0	0	0
2	0	0	1
3	0	1	0
4	0	1	1
5	1	0	0
6	1	0	1
7	1	1	0
8	1	1	1

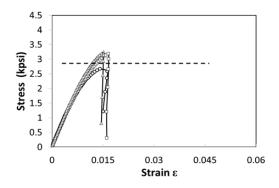
Figure 1. Samples of various lattice structures made using binder jetting-based ExOne M-lab.



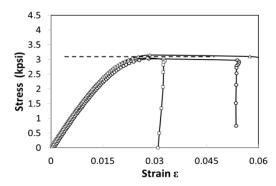
Results and Discussion

Parameter and Property Analysis of PLA

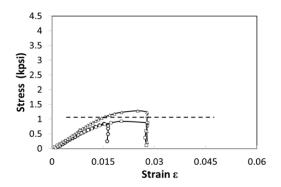
Tensile strength was tested for all of the PLA samples using the MTS 810 tester. Figure 2 shows the stress-strain curves of the PLA material for the nine trials.

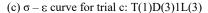


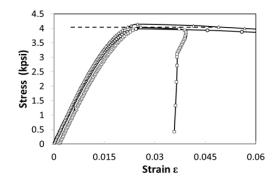
(a) $\sigma - \epsilon$ curve for trial a: T(1)D(1)1L(1)



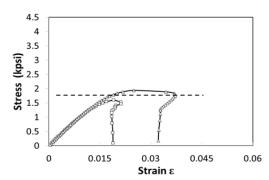
(b) $\sigma - \varepsilon$ curve for trial b: T(1)D(2)1L(2)



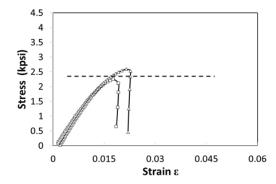




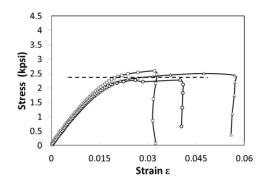
(d) $\sigma - \varepsilon$ curve for trial d: T(2)D(1)1L(2)



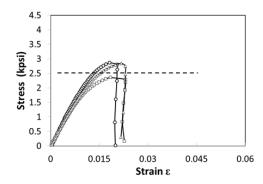
(e) $\sigma - \varepsilon$ curve for trial e: T(2)D(2)1L(3)



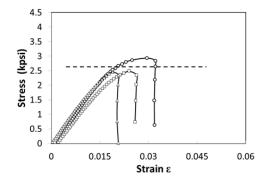
(f) $\sigma - \varepsilon$ curve for trial f: T(2)D(3)1L(1)



(g) $\sigma - \varepsilon$ curve for trial g: T(3)D(1)1L(3)



(h) $\sigma - \varepsilon$ curve for trial h: T(3)D(2)1L(1)



(i) $\sigma - \varepsilon$ curve for trial i: T(3)D(3)1L(2)

Figure 2. Stress-strain curves of the PLA material tested using the MTS tester.

The stress-stain curves showed that the samples for each trial were consistent, from a strength point of view, although minor variations from sample to sample existed. An average had to be taken in order to represent the tensile strength of each trial, as indicated by the dotted line in each graph. It was clear that the configurations of building parameters affect strength. For the tested cases, the strength of the parts varied from about 1 ksi to 4 ksi. The difference was significant. These observations indicated that the factors and their corresponding levels may be optimized for achieving desirable material properties. It can be concluded that a medium process temperature (225°C), low deposition rate (30 mm/s),

and medium layer thickness (0.13 mm) represent the optimized design configuration for producing the highest tensile strength for the PLA material using the specific 3D printing machine, Ultimaker 2. To generalize, this may apply to all fused deposition-based 3D printing processes with similar principles, though the exact temperature, deposition rate, and layer thickness may vary depending on the specific machine.

Property and Processing Parameter Analysis of Stainless Steel 316

To study the effect of the design parameters on metal and metal alloy materials, stainless steel 316 was chosen, due to its broad applications. Compression testing on the samples was done according to ASTM E9 standards for metallic materials. The MTS 810 material testing system with a 1 KN load cell at a constant crosshead speed of 0.1 in/min was used and the data were recorded every 0.05 seconds. Table 4 shows the compressive strength and shrinkage of the experimental samples. The compressive strength ranged from 82.89 MPa to 1780.5 MPa; the radial shrinkage ranged from 0.06% to 3.72%; and, the longitudinal shrinkage ranged from 0% to 2.945%. These observations show that the process parameters, layer thickness, sintering time, and sintering temperature can significantly affect the compressive strength and shrinkage of the fabricated stainless steel 316 part, and optimal higher strength of the part can be achieved through control of the processing parameters.

Table 4. Experimental results of compressive strength and shrinkage of the samples.

#	A	В	С	Compressive Strength (Mpa)	Radial Shrinkage (%)	Longitudinal Shrinkage (%)
1	0	0	0	745.5	0.363	1.525
2	0	0	1	1780.5	1.99	2.395
3	0	1	0	1811	2.97	2.53
4	0	1	1	1972	3.72	2.685
5	1	0	0	82.89	0.06	-0.1
6	1	0	1	879.5	2.71	1.86
7	1	1	0	978.5	2.30	2.045
8	1	1	1	1083.5	2.55	2.945

Figure 3 shows the effects of the processing parameters and their corresponding levels to the compressive strength of the samples. The plot graphically displays the average output value of the compressive strength for multiple levels of a given input. It also shows the effect of various parameters and their levels on average compressive strength. From

Figure 3, it is clear that low layer thickness, longer sintering time, and higher temperature lead to significantly higher compressive strength of the stainless steel part. Longer sintering time and higher temperature can also be used to improve strength of the part. Sintering is a diffusion-controlled process, where reduction of free space operates as a driving force; the solid mass is created by atoms diffusing across the particle boundaries. With the increase in sintering time and sintering temperature, particles connected closer; thus, the structure became stronger and more compact, providing higher compressive strength. Compressive strength increased with an increase in sintering parameter values.

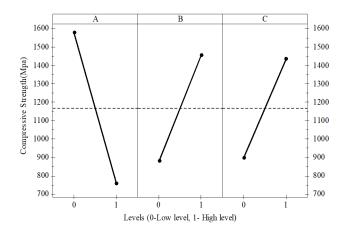
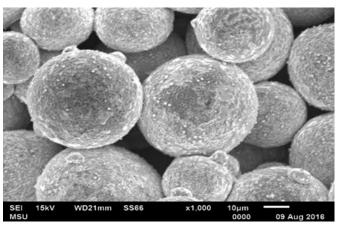


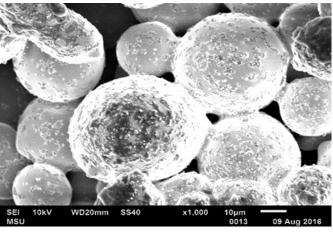
Figure 3. Effects plot of process parameters on compressive strength: A, layer thickness (low [0], 50 μ m; high [1], 100 μ m); B, sintering time (low [0], 2 hours; high [1], 4 hours); C-Sintering temperature (low [0], 1120° C; high [1], 1180° C).

This phenomenon may be explained by looking at micro images showing the fusion; Figure 4 displays micro images made by a scanning electron microscope (SEM). The images were produced by scanning electron microscope JEOL JSM-6510MV. Figure 4(a) shows the SEM image of the sample with two hours sintering time and sintering at 1120°C, while Figure 4(b) represents four hours of sintering time with sintering at 1180°C. It is clear that longer sintering time and higher sintering temperature lead to larger and wider fusion zones, which indicates that atomic diffusion is greater and deeper. As a result, particle bonding is between stronger and much stronger.

From the observations made based on the studies on PLA polymer material using FDM 3D printing and the studies on stainless steel 316 using the binder jetting 3D printing method, design parameters play significant roles. The configuration of the parameters can dramatically change the final product's mechanical properties. Even though the material is the same at the starting point, the process used in fabrication may change the properties. The process design parameters and their levels may be optimized in order to obtain desirable final material properties.



(a) Two hours at 1120°C



(b) Four hours at 1180°C

Figure 4. SEM images of samples made at sintering time and temperature.

Conclusions

The studies on PLA polymer using the fused deposition method and stainless steel 316 with the binder jetting method were presented. The process design parameters and their corresponding various levels were studied. Tensile strength for the PLA polymer material and compressive stress for stainless steel 316 were studied. It was found that the design parameters and their corresponding levels for obtaining desirable mechanical properties can be optimized for both cases. For the PLA material, medium process temperature, low deposition rate, and medium layer thickness represented the optimal design configuration for producing the highest tensile strength. For stainless steel 316, cylindrical samples were fabricated for each run of the experimental plan with different process parameters. Sintering time, sintering temperature, and layer thickness were analyzed for their effects on compressive strength. The optimal responses considered in the study were high compressive strength and low radial

and longitudinal shrinkage rates. The optimal parameters for high compressive strength were low layer thickness, longer sintering time, and higher sintering temperature, because the latter two lead to a larger, wider fusion zone. This indicates that atomic diffusion is greater and deeper, and the fusion zone forms a larger portion if the layer is thinner. The identified optimal parameters might not be the same for different materials, but the study serves as a guide for adjusting printing parameters for different materials.

Although the technologies involved in AM 3D printing are different, the principles of adding layers are the same, and it is clear that the design parameters and their levels may significantly affect the properties of the final part. To design and fabricate a part with specific materials, its mechanical properties may be optimized through appropriate control of the processing parameters and their levels. Future studies can be conducted on more parameters at more levels using structural design analysis to provide yet more insight into design materials and structures with this important manufacturing method.

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Mechanistic Implications of Mouthpiece Design Geometry and Powder Mixture Homogeneities on Successful Generation of Aerosolized Submicron Particles from Respiratory Drug Delivery Devices

Mohammed Ali, the University of Texas at Tyler

Abstract

In this paper, the author presents the mouthpiece design geometry and powder mixture homogeneity effects of three respiratory drug delivery devices (RDDDs) to the aerodynamic and electromechanical properties of generated inhalable submicron particles. These devices are commonly known as dry-powder inhalers (DPIs). Currently, DPI is considered as the preferred type of pulmonary drug administration device with the greatest potential for other biomedical applications. The generation and inhalation of aerosolized submicron particles from the DPIs gained much attention in the late 1980s, when the Montreal protocol was designed to discourage production of chlorofluorocarbon (CFC) propellant, a widely used aerosolization component in the popular metered dose inhaler.

Montreal protocol on controlling ozone depleted CFC chemicals became a major drive for the design and manufacturing technology of the DPI. The successful delivery of drugs deep into the lungs depends on various aerodynamic and electromechanical properties of generated particles from the devices. Effects of the mechanistic behaviors of the DPI design geometry, and integration between device performance and powder formulations are prime subjects for investigation. An electronic single-particle aerodynamic relaxation time analyzer, which functions on the laser Doppler velocimetry principal, was employed in order to measure submicron particles' charge and size in real time.

Results revealed that the generated aerosol particles from all three DPIs were found to not only have different size distributions but also varied in their charge distributions. The net charge-to-mass ratio of DPI 1, 2, and 3 particles were 3.80 $\mu\text{C/g}$, 1.37 $\mu\text{C/g}$, and 1.45 $\mu\text{C/g}$, respectively. Count and mass distributions of the particles were reproducible (p<0.05) for all DPIs. Variations in electrical, mechanical, and aerodynamic properties of the DPI aerosols can be explained by the combined effects of triboelectrification charging between carrier and active drug powders, delivery device geometries, polymeric material surfaces of delivery devices, and drug/carrier homogeneities.

Introduction

Dry-powder inhalers (DPIs) are a popular type of respiratory drug delivery device (RDDD), which generates an inhalable aerosolized particulate form of medications for the treatment of asthma and chronic obstructive pulmonary disease. The generation and inhalation of aerosolized fine and ultrafine particles from the DPIs gained much attention in the late 1980s, when the Montreal protocol was designed to discourage production of CFC propellant, a widely used aerosolization component in the popular metered dose inhaler (WMO, 2018). The Montreal protocol, on controlling ozone depleted CFC chemicals, became a major drive for the design and manufacturing of the DPI (de Boer et al., 2017). DPIs are breath-actuated devices, requiring inspiratory flow rates of 30-130 L/min to successfully generate an aerosolized bolus of drug/carrier powders (Labiris & Dolovich, 2003). The manufacturing technologies related to DPI drug dose preparation and releasing techniques and mouthpiece geometries have been constantly improved in order to fulfill the requirements of the biomedical device industry. The device features have consequential relationships with the emitted drug/carrier powder aerosol properties. The successful delivery of drugs deep into the lung depends on various aerodynamic and electromechanical properties of generated particles. Precise quantification of these properties is not only convincing but also serve as a guide for better manufacturing techniques to satisfy the growing RDDD industry (BCC Research, 2018).

Mathematical Simulation on DPI Mouthpiece and Aerosol Generation

Numerical and computational fluid dynamics (CFD) modeling studies have quasi-successfully predicted the respiratory aerosol flow and generation from the DPI mouthpiece inlets. Huynh et al. (2015) adopted the Boltzmann sigmoidal modified function (see Equation 1) to determine the rate of emptying of powder formulations from the DPIs. Additionally, they used a laser diffraction apparatus to determine the powder concentration of the aerosolized sample. The aerosolized sample defined as laser light intensity reduction (or obscuration) in the apparatus's measurement cell is used as a function of aerosolization time.

$$y(t) = \frac{\%PO}{1 + \exp\left\{-\left[\frac{t - t_{50}}{t_{empty}}\right]\right\}}$$
(1)

where, %PO is the peak calculated obscuration value in percentage form; t_{50} is the time taken to reach half of %PO in seconds; and, t_{empty} is the slope of the function, with a larger t_{empty} value indicating a slower emptying behavior of the inhaler.

Results showed that the increase in powder residence time inside the inhaler increases the interaction among the dispersed powder, air-stream, and device walls. This action potentially affected the powder-release behavior and subsequent dispersion performance. In the assessment of DPI powder de-agglomeration behaviors, mathematical modeling plays a key role in the interpretation of the powder release from DPI systems (Huynh et al., 2015). Another study adopted the Reynolds-Averaged Navier-Stokes equation (or RANS equation) for idealized mouth geometry to understand aerosol flow and deposition from the DPI mouthpieces (Ilie, Matida, & Finlay, 2008). A good agreement was found when compared with experimentally measured data. The RANS is a time-averaged mass conservation equation of motion for the aerosolized form of turbulent fluid flow through DPI devices, which can be described by Equation 2:

$$\rho \overline{u}_{j} \frac{\partial \overline{u}_{i}}{\partial x_{j}} = \rho \overline{f}_{i} + \frac{\partial}{\partial x_{j}} \left[-\overline{p} \delta_{ij} + \mu \left(\frac{\partial \overline{u}_{i}}{\partial x_{j}} + \frac{\partial \overline{u}_{i}}{\partial x_{i}} \right) - \rho \overline{u'_{i} u'_{j}} \right]$$
(2)

where, u, \bar{u} , and u represent the instantaneous, mean, and fluctuating terms of aerosol flow velocity, respectively; \bar{p} is the mean pressure; \bar{f}_i is a vector representing external forces; μ is dynamic viscosity; and, x_i and x_j are position vectors

The basic tool required for the derivation of the RANS equations from the instantaneous Navier-Stokes equations is the Reynolds decomposition of flow velocity (Anderson, 2009). Reynolds decomposition refers to the separation of the flow variable (like velocity u) into the mean (timeaveraged) component (\bar{u}) and the fluctuating component (\dot{u}) . Due to the fact that the mean operator is a Reynolds operator, it has a set of properties. One of these properties is that the mean of the fluctuating quantity is equal to zero ($\dot{u} = 0$). All of these studies concluded that the application of CFD in the design of mouthpieces as well as DPI is often difficult, due to the highly complex nature of aerosol generation from drug-carrier powders. However, they do provide valuable insight into certain aspects of device performance. Moreover, computing power becomes limited when it requires the implementation of numerical methods to the DPI design. Yet, the most useful application of CFD usually happens when concurrent CFD and experimental results are analyzed.

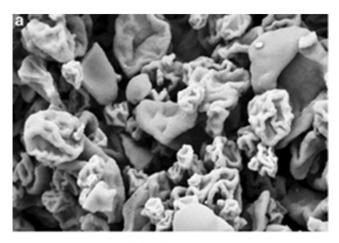
Design Implications to Particle Aerodynamic Size and Electrostatic Charge

Typically, DPI products consist of a drug formulation (the drug constituent part) and a container closure system. DPI drug formulation contains the drug substance and carrier excipients (e.g., lactose), which provides for uniformity and flow-ability of a blend during manufacturing. Carriers can also enhance the reproducibility of the metered, fine-particle dose by reducing agglomeration of the drug substance. A DPI container closure system consists of the device constituent part (DCP) and any protective secondary packaging (e.g., an overwrap). The materials used to fabricate the DCP may come in direct contact with either the formulation or the patient, thereby potentially affecting product safety and performance. For instance, drug particle-surface interactions, such as adhesion of drug onto mouthpiece surfaces, can affect the delivered dose drug/carrier homogeneities, aerodynamic particle size distribution, and the particles electrostatic charge distributions.

The DCP of an RDDD acts as the delivery system of the drug, its design, geometry, and dimensions. This can influence device resistance, air flow, shear, and turbulence generated within the DCP. The Food and Drug Administration recommends that RDDD manufacturers use experimental and modeling studies on their formulations, production processes, and DCP designs. This is recommended in order to identify the quality target product profile, critical quality attributes, and potential risks to the product, and then initiate product and process development to define a control strategy that eliminates or mitigates the risks (FDA, 2018). In DPI carrier-drug formulation, particular interactions within the formulation govern both the drug dissociation from carrier particles and the disaggregation of the drug into primary particles with a capacity to generate respirable (aerodynamic diameter or size, d_a , range from 0.5 μ m to 10 µm) and penetrable deep into the lungs. Formulations must achieve two challenging characteristics: adhesion between carrier and drug must be sufficient for the blend to be stable, yet weak enough to enable release of the drug from the carrier during patient inhalation.

Also, to be enabled as a consistent dose while metering inside the DPI device, the drug-carrier powders must have flow properties. In addition, the powder should be capable of de-agglomerating while flowing in air-stream, and the inter-particulate interaction of inhalation powders needs to be understood in order to advance DPI formulation. Particle engineering technology demonstrated that highly irregular carrier particles with relatively large geometric diameters disperse readily, due to limited surface contact points with drug particles (see Figure 1). Reports from experimental studies found in the literature established that respiratory powdered drug particles aerosolized from DPIs may charge electrostatically (Ali, Mazumder, & Martonen, 2009). These particles acquire charge via electron and ion transfer during

particle-particle and particle-device component contact and separation. The charge distributions (both magnitude and polarity) are dependent on: 1) work functions of the materials coming in contact with each other; 2) the friction and surface area involved in the contact; and, 3) dielectric properties of the materials and the ambient relative humidity (Crowley, 1999). The charge magnitude is affected by numerous factors including the powdered drug's chemical structures, the delivery device's internal air flow paths, the drug-carrier mixture's in-homogeneities, and their particle size distributions (Byron, Peart, & Staniforth, 1997).



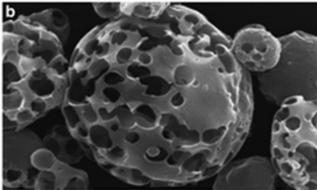


Figure 1. Drug and carrier particles harvested from DPIs. Drug particles attracted to carrier particles. Reprinted with permission.

Large particles ($d_a > 4 \mu m$) have a low charge-to-mass ratio (q/m), and their depositions are dominated by inertial impaction, whereas smaller particles ($d_a < 4 \mu m$) achieve higher charge-to-mass ratios and their depositions are dominated by both space and image charge forces (Ali, Reddy, & Mazumder, 2008). A space charge force is the result of mutual repulsion between particles of like charge. Image force is the attraction between the charged particle and conductive respiratory airway wall, which affects single particles and increases as a particle gets closer to the wall. Proper quantification of the aerodynamic diameter or size (d_a) and electrostatic charge (q) upon generation as a bolus of aerosol is

necessary. Such understanding will enable present powder formulations and manufacturing technology to address the drug's shear force and tribo-charging involved in dispersing from excipient. So the objective of this experimental investigation was to quantify the electrostatic charge and aerodynamic size distribution of the drug particles generated by three DPIs. An electronic single-particle aerodynamic relaxation time analyzer (ESPARTA), which functions on the laser Doppler velocimetry principle, was employed in order to measure submicron and nanoparticle charge and size in real time.

Materials and Methodology

Three commercially available DPIs were used in this study. In order to avoid perceptions among marketed DPI products, this study adopted generalized naming: DPI-1, DPI-2, and DPI-3. The scope of this study was to understand the manufacturing and design effects on aerosol electro-aerodynamic-mechanical properties rather than on their commercial or therapeutic performances. All of these powdered drug formulations contained both carriers and active pharmaceutical ingredients.

DPI-1 Working Principle and Use

DPI-1 was a Handihaler type of device, which is marketed in usable patient ready form. For the dry-powder aerosol formation from this DPI, a drug capsule was placed into the center chamber of the Handihaler device. The capsule was pierced by pressing and releasing the green button on the side of the device. The drug formulation along with its carrier particles was dispersed into the air stream when the patient inhaled through the mouthpiece. Because there was not a dose counter on this DPI, doses had to be tracked manually. The standard operation of use of DPI-1 included: 1) opening the dust cap and mouthpiece; 2) removing one drug capsule from its package and separating the blister strip; 3) placing the capsule in the center chamber and closing the mouthpiece firmly until a click is heard; 4) piercing the capsule by pressing the green button; and, 5) closing the patient's lips tightly around the mouthpiece and inhaling one bolus of aerosol stream.

DPI-2 Working Principle and Use

DPI-2 was a Diskus type inhaler device, which is marketed in usable patient ready. The coil dosing strip contains 60 individual foil blisters. A mechanism pierces the blister when the patient opens the mouthpiece cover of the device before each dose. This action makes the powder available for inhalation. The standard operation of DPI-2 included: 1) holding the device at a flat, level position and rotating the mouthpiece cover; 2) sliding the lever to advance the next blister and making sure the lever is firmly clicked into the place; and, 3) closing patient's lips tightly around the mouthpiece and inhaling one bolus of aerosol stream.

DPI-3 Working Principle and Use

DPI-3 was a Turbuhaler type device in usable patient ready form. This kind of DPI contains a reservoir of 200 doses of drug-carrier powders. For each dose to be inhaled as a bolus of aerosol, it is necessary to twist the grip at the base of the device to rotate a disk contained of small cylinders. Those disks are filled with powder from the reservoir. The standard operation of DPI-3 included: 1) holding the inhaler in an upright position; 2) twisting the brown grip as far as it will go in one direction; 3) twisting the grip all the way back in the other direction; and, 4) inhale one bolus of aerosol stream. The cohesive nature of inhalation of aerosolized powders makes it necessary to impart significant energy to the mouthpiece to efficiently disperse and deagglomerate the powder so that sufficient aerosol will be generated and inhaled in order to achieve a therapeutic advantage (Stein & Thiel, 2017).

Experimental Setup

The electronic single-particle aerodynamic relaxation time analyzer (ESPARTA) was used to determine the DPIgenerated particles in real time. In characterizing aerosolized submicron particles, the laser Doppler velocimetry (LDV) technique is a popular method. Optoelectronic measurements, including LDV, are non-intrusive and have fast response times and high data measurement accuracy. Furthermore, there has been a tremendous amount of interest and success in the real-time analysis of aerosols upon generation. ESPARTA incorporates the methodology of the LDV principle, which measures simultaneously both aerodynamic diameter and electrostatic charge (magnitude and polarity) of DPI aerosol particles. Its application in the area of RDDDs was demonstrated elsewhere (Ali et al., 2009; Mazumder, Wilson, & Wankum, 1989). The suction pump of the ESPARTA-sampled aerosol occurred at the rate of 1 L/ min (through aerosol inlet). The flow was directed downwards through a sensing volume of concentrated beams of laser radiation.

During sampling, each particle traveled through converging laser beams and experienced AC electrical excitation, which made it oscillate horizontally. A photomultiplier was used to measure the intensity of the scattered light generated by each particle as it passed through the sensing volume. The electronic signal and data processor analyzed the phase lag of the particle's motion with respect to the AC electrical field driving the particle. The aerodynamic size was derived from the phase lag value. The direction and amplitude of the electrical migration velocity of the particle with respect to the electrical field provided the polarity and magnitude of its electrostatic charge. Figure 2 illustrates the schematic effects of the experimental setup. ESPARTA operates in two modes, as per its design and working principle. In mode 1, it measures the aerodynamic size of each particle and whether the particle is charged or uncharged. Acquired aerosol data in this mode represents total (charged and uncharged) particles. In mode 2, it measures the aerodynamic size and the electrostatic charge of each charged particle. In mode 2, it also ignores, by design, the uncharged particles. In this study, mode 1 and mode 2 data were obtained in completely separate experimental runs. Figure 2 shows how an aerosol holding chamber (AHC) held aerosols for characterization.

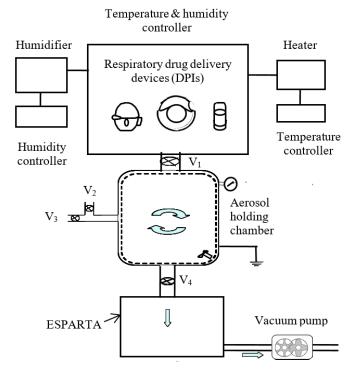


Figure 2. Schematic of the experimental arrangement designed to measure electrostatic charges and aerodynamic diameters of RDDD aerosol particles in real time.

The AHC has a volume of 28.3 liters and four ports equipped with valves (V_1 , V_2 , V_3 , and V_4), and one pressure gauge. Valve V_1 controls the inhalation of drug aerosol to the chamber, V_3 connects the chamber to a vacuum pump, V_2 opens the chamber to ambient air, and V_4 controls aerosol flow from the chamber to the ESPARTA analyzer. The Aneroid pressure gauge monitors the chamber's vacuum pressure. Furthermore, a battery-operated fan was placed inside the AHC in order to maintain circulation and help prevent the aerosol from settling. The walls of the inside chamber were lined with a grounded wire mesh to discharge any static electricity that may have been acquired by the chamber's wall. Above all, this device helped to conduct this experiment methodically.

During each experiment, the aerosol holding chamber was evacuated down to 36 cm of mercury. This was done so that a bolus of four liters of aerosol could be drawn from the test DPIs upon opening of valve V_1 at a rate of 30 L/min for a

period of eight seconds (30 L/min x 8 s = 4.0 L). The concept of 4L inhalation is a recommendation by the FDA (2018). The flow rate was determined using an Extech heavy duty hot wire thermo-anemometer (Extech Instruments, n.d.). To characterize DPI aerosols, RDDD scientists agreed that bolus inhalations be employed in order to comply with standard operating conditions. For that reason, the author of this current study adopted this methodology. A humidity-controlled chamber was used to preserve a constant relative humidity (RH) in the AHC. The inhalation experiments with all DPIs were conducted by holding them in the top opening of valve V₁. Hence, the inhalation of bolus aerosol through V₁, while the DPI was placed inside the humidity-and temperature-controlled chamber along with sampling from the AHC, was done purposely to simulate the temperature and humidity inside a patient's mouth. The constant temperature and humidity were maintained by an Electro-tech Systems 5100-240 controller (Electro-tech Systems, n.d.) at 37°C and 95%, respectively.

Evacuation of the AHC and inhalation of a total of 4L of drug/carrier powder aerosols was done in order to comply with DPI drug administration to a COPD adult patient. The AHC was cleaned before each run of the experiment. The DPI devices were made ready for inhalation as per standard operating procedures described in the Materials and Methodology section. The DPI mouthpieces were placed at inlet valve V_1 just before opening it. Once the AHC was filled, valves V₁, V₂, and V₃ were closed and the circulation fan started. Valve V₄ was then opened for sampling by the ES-PARTA for a period of five minutes. Thus, it was unlikely that variation in the quantity of the drug/carrier powder in each dose of the individual DPI affected the measurements. Also, comparisons of the portion of charged particles in each bolus were not affected. The repetitive procedure was continued for five consecutive runs. Aerodynamic size and electrostatic charge distribution were measured in each case.

Results and Discussion

The cost in 2015 for the respiratory drug manufacturing industry to market medications for such ailments as asthma and COPD was \$9.9 billion. This final cost analysis includes the countries of Italy, Spain, France, Germany, the United States, the United Kingdom, Japan, and Australia. In 2025, the estimated cost from those same countries is expected to increase by \$14.1 billion, bringing the estimated total for 2025 to \$24 billion. This represents a compound annual growth rate of 3.7%, according to the research and consulting firm Global Data (2017). As a result, there is a growing demand for dry-powder inhalation formulations that allow for composite-particle technology to have the development of more efficient formulations and challenging molecules. Spray drying is an enabling technology for composite-particle preparation (Santos et al., 2018). It is also ideal for generating engineered particles with improved electromechanical and aerodynamic performance. During

spray drying, a solution of the drug substance and suitable carrier excipients are subjected to mild flash drying, which allows for careful control of particle properties (particle size, bulk density, degree of crystallinity, etc.) (Winters & Costa, 2016).

Storage location and moisture affect the flow and deagglomeration of DPI drug/carrier powder mixtures. Although there is no clear evidence about the DPI cleaning practice, each manufacturing company has recommendations for periodic cleaning, and suggests wiping the mouth-piece of the DPI with a clean dry cloth. In this study the author adopted these procedures. Tables 1 and 2 summarize the aerodynamic size, count median aerodynamic diameter (CMAD), mass median aerodynamic diameter (MMAD), and electrostatic charge results of three DPIs.

Table 1. Summary of the three dry-powder inhaler (DPI) aerosols aerodynamic size properties (mean \pm SD).

DPI	CMAD (μm) (mean ± SD)	$\begin{array}{c} MMAD \ (\mu m) \\ (mean \pm SD) \end{array}$
DPI 1	3.61 ± 0.07	4.99 ± 0.03
DPI 2	3.61 ± 0.19	5.29 ± 0.15
DPI 3	2.86 ± 0.02	3.65 ± 0.10
CMAD: Count median aerodynamic diameter, MMAD: Mass median aerodynamic diameter		

Table 2. Summary of the three dry-powder inhaler (DPI) aerosols electrostatic charge properties (mean \pm SD).

DPI	$ \begin{array}{c ccc} Charged & + \ ve \ Counts & Charge/mass \\ Particle & vs & + \ ve \ and \\ \% & - \ ve \ Counts & - \ ve \ (\mu C/g) \\ \end{array} $		Net Charge/ mass ratio (μC/g)	
DPI 1	62 ± 4	$1783 \pm 20 \\ 1899 \pm 24$	+ 5.30 ± 14 - 6.61 ± 16	$+3.80 \pm 06$
DPI 2	67 ± 5	$1626 \pm 29 \\ 2313 \pm 31$	+ 4.77 ± 13 - 6.30 ± 17	+ 1.37 ± 03
DPI 3	28 ± 2	475 ± 9 618 ± 12	+ 5.41 ± 11 - 6.63 ± 12	+ 1.45 ± 04

It is necessary to mention here that the data presented in these tables represent the normalized data (mean \pm SD) from five runs of sampled aerosol particle counts (Bruna, Fourment, & Stradella, 2000; Srinivasan et al., 2018). According to the ESPARTA working principle, the uncharged particle counts are the difference between total particles and charged particles. It was observed that the aerosol particles generated from all three DPIs were found to not only have different size distributions, but also varied in their charge distributions. The net charge-to-mass ratio of DPI 1, 2, and 3 particles were 3.80 $\mu\text{C/g}, 1.37~\mu\text{C/g},$ and 1.45 $\mu\text{C/g},$ respectively.

Figure 3 shows the graphical representations of the CMAD and MMAD for all three DPIs. Count and mass distributions were reproducible (p<0.05) for each of them. According to the guide for aerosol delivery devices published by the American Association of Respiratory Care (2013), particles in the size range of 1-5 μ m are able to reach the lung periphery. In this respect, data in Tables 1 and 2 along with Figure 3 tell us that all three DPIs were producing acceptable levels, according to the respiratory drug industry, and therapeutically capable size range drug/carrier mixture of particles (American Association of Respiratory Care, 2013).

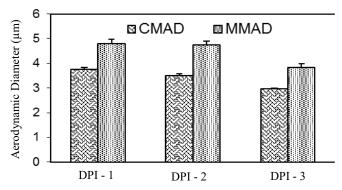


Figure 3. Count median aerodynamic diameter (CMAD) and mass median aerodynamic diameter (MMAD) of three DPIs.

Figure 4 shows the aerodynamic size distributions of the submicron drug aerosol particles from the three DPIs. The particle-size distributions of all DPI aerosols were fairly constant within the respirable range (0.5-10 μm) and aerodynamically were monodispersed. This property makes these pharmaceutical drug aerosols therapeutically acceptable. Since the performance of an inhaled formulation depends greatly on particle aerodynamic size distribution (PASD), increasing the number of fine particles in the carrier can improve the aerosolization of the active drug ingredient. In addition, the effect of PASD on a bulk powder is also broadly understood in terms of powder flow. Figures 3 and 4 show the PASD results, which demonstrate that an experimental design approach can be used successfully to support dry-powder formulation development as well.

Figure 5 shows the real-time electrostatic charge distributions of all three DPIs. From the data in Table 2 and Figure 5, it can be seen that the charged particles in the DPI-1-generated aerosols were 62%, of which 48% were positively charged and 52% were negatively charged. Similarly, the DPI-2-generated aerosols were 67% charged, of which 41% were positively charged and 59% were negatively charged. The DPI-3-generated aerosols had 28% charged particles of which 43% and 57% were charged positively and negatively, respectively. Such observations are further confirmed by inherent net charge-to-mass ratio data in Table 2, where DPI-1 showed the highest (+3.80 \pm 0.06 μ C/g) and DPI-2 showed the lowest (+1.37 \pm 0.03 μ C/g).

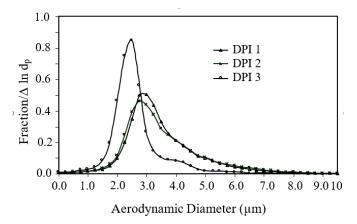


Figure 4. Real-time aerodynamic size distributions of submicron drug aerosol particles of three DPIs.

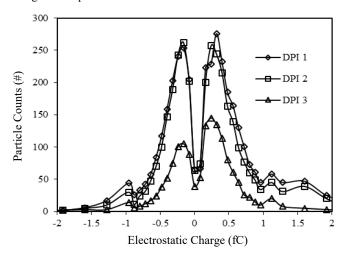


Figure 5. Real-time electrostatic charge distributions of submicron drug aerosol particles of three DPIs.

Interestingly, the proportion of charged particles for DPI-3 was lowest (28%), and its net charge-to-mass ratio (+1.45 \pm 4) was very close to that of DPI-2 (+1.37 \pm 0.03 $\mu\text{C/g}$). This information gives us two possibilities for the electromagnetic effects of DPI aerosols: a) more particles from DPI-1 will be likely to be deposited in the conducting airways of the lung, and b) the DPI-2 and -3 particles are more likely to experience less space and image charge forces while flowing though the conducting airway and experience greater deposition in the distal regions of the lung.

Overall, the findings presented in Tables 1 and 2, Figures 3-5, and the variations in electrical, mechanical, and aerodynamic properties of the DPI aerosols can be explained by the combined effects of triboelectrification charging between carrier and active drug powders, delivery device geometries, polymeric material surfaces of delivery devices, and drug/carrier homogeneities.

For carrier formulations, the particle-size distribution of the drug powders and the percentage of fine lactose in a formulation are the main parameters that influence aerodynamic performance. In addition, the formulation has a significant impact on blending and capsule-filling yields. Specifically, formulations that enable improved fine-particle fractions are detrimental to the process yield, leading to significant product loss in the blending and capsule-filling steps. As a result, there is a need to balance the desired aerodynamic performance with the manufacturability properties of any given DPI formulation. Specifically for carrier formulations, whenever possible, the fine lactose percentage should be minimized to <10% and low fill weights of <10 mg should be avoided in order to achieve the best balance between manufacturability and aerodynamic performance (Winters & Costa, 2016).

Polymeric materials for manufacturing RDDDs have been promising for some time. However, selecting the best material for the parts and devices is needed in order to make new products functional and safe. In this study, it was found that the material provides a considerable impact on device performance. Moreover, when the device being developed has unique requirements, developers must consider what material will have the necessary mechanical, electrical, and biological properties that will allow its use at the lowest possible cost. Czuba (2015) suggested a group of such polymers, including polyether ether ketone, polyethylene and cyclic olefin copolymers, bioresorbables, and fluoropolymers.

At this point, it is necessary to recognize certain limitations in this study. For example, this current study only addressed the therapeutically useful fraction of RDDD-emitted aerosol particle sizes in the range of 0.5 to 10 µm. Additionally, this study purposely avoided considering the electroaerodynamic behavior of particles smaller than 0.5 µm, because ESPARTA was not able to detect sizes below this range. The maximum counting limit of this instrument was 200 particles per second. Also, it was assumed that aerodynamic properties such as diffusion, aggregation, and sedimentation of aerosols in the sampling chamber were unchanged during five minutes of sampling period, and that they were dynamic in the chamber.

Like other real-time single-particle counting instruments, ESPARTA also suffers coincidence effects, which occur when more than one particle is present in the instrument's measuring volume. This can distort sizing information and lead to underreporting of particle concentration. It is one of the reasons the ESPARTA samples aerosol at a rate of 1.0 L/min by design. Furthermore, it was beyond the methodology of this study, whether the assessment was done only for the non-active drug carrier with active drug powders for the tested DPIs or not. However, the fundamental assumption of a DPI-emitted powder in the inhaled air is that each aerosol particle may contain both drug and carrier.

Conclusions

This study presented a new method of real-time and simultaneous measurement of the aerodynamic size and electrostatic charge of the respiratory drug DPI- emitted bolus aerosol particles. Aerosols generated by all three devices tested (number of runs, n = 5) exhibited net electro-positively charged particles. These DPIs were not only capable of producing particles of different size distributions but also varied charge distributions. Therefore, the author believes that the findings have practical values and biomedical device manufacturing implications, and suggests that the developers of RDDDs consider electrodynamic effects, while designing improved products. Limitations of this study included: 1) the particle size range only included those between 0.5 and 10 µm; 2) ESPARTA's maximum particle counts were 200 per second at a rate of 1.0 L/min by design; and, 3) the fundamental assumption was that the DPI-emitted powders contained both drug and carrier.

Acknowledgements

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Biography

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ENHANCING DOWNSTREAM PERFORMANCE OF 5G Mobile Fronthaul

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Abstract

5G mobile fronthaul (MFH) requires the support of a fiber -based infrastructure such as a time division multiplexing-passive optical network (TDM-PON). Due to centralization in TDM-PON, typically the central office (CO) is responsible for both the upstream and downstream bandwidth allocation tasks. The upstream TDM-PON task consumes the network resources, which hinders the downstream MFH performance. Therefore, to improve the downstream MFH performance, the authors propose a TDM-PON scheme that transfers the centralized upstream task from the CO to the wireless nodes close to the customer end. Consequently, CO resources are freed up in order to address the downstream tasks, which paves the way for enhanced downstream MFH performance.

Introduction

The unparalleled interconnection among wireless devices requires virtually unlimited bandwidth and very low latency. To meet such a requirement, a new networking concept beyond 4G is envisioned, namely 5G. Its expectations and stringent requirements necessitate advanced technologies, such as exploitation of unused high-frequency bands (mm Wave), smaller cells, cell densification, massive multiple input multiple output, etc. (Andrews, Buzzi, Choi, Hanly, Lozano, Soong, & Zhang, 2014; Alimi, Teixeria, & Monteiro, 2018). One of the important segments of the 5G network is the radio access network (RAN), which wirelessly connects user equipment to the core network through the base stations (BSs). Traditional BSs are composed of two key elements: the base band unit (BBU) and the remote radio head (RRH). The BBU is responsible for digital signal processing and the RRH, which is connected to an antenna, is responsible for transmitting and receiving radio frequencies (RF).

There are two types of RAN architectures in terms of the configuration of BBUs and RRHs: the distributed-RAN (D-RAN) and the centralized-RAN (C-RAN). The D-RAN integrates the BBU and RRH into the antenna site in order to function as a single unit. On the other hand, the C-RAN places the two elements at separate locations, while the BBU is centralized at a location (e.g., CO) away from the RRH (at the antenna site). Figure 1 shows how they are connected via a network known as the mobile fronthaul (MFH) (Andrews et al., 2014; Alimi et al., 2018; Pizzinat, Chanclou, Diallo, & Saliou, 2015). The C-RAN offers efficiency via the centralization of the BBUs, which allows the sharing

of the backplanes along with computational and maintenance resources. Additionally, it facilitates RAN performance enhancement via inter-cell interference coordination and coordinated multipoint transmission/reception. It also simplifies antenna site designs by shifting system complexity and cost towards the MFH (Rost et al., 2014; Haberland, Derakhshan, Grob-Lipski, Klotsche, Rehm, Schefczik, & Soellner, 2013; Sundaresan, Arslan, Singh, Rangarajan, & Krishnamurthy, 2015).

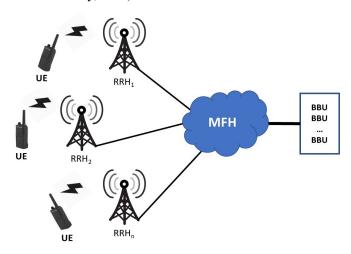


Figure 1. 5G mobile fronthaul.

The massive volume of MFH traffic and its strict latency requirement is difficult to imagine without the support of a fiber network infrastructure. Among the various fibersupported networks, the passive optical network (PON) is still the most economical choice for MFH (Shibata, Tashiro, Kuwano, Yuki, Fukada, & Terada, 2015; Zhou, Liu, Effenberger, & Chao, 2018; Anthapadmanabhan, Walid, & Pfeiffer, 2015; Shibata Tashiro, Kuwano, Yuki, Terada, Otaka, 2015; Kobayashi, Hisano, Shimada, Terada, & Otaka, 2016; Tashiro, Kuwano, Terada, Kawamura, Tanaka, Shigematsu, & Yoshimoto, 2014). The PON can be of two major types, time division multiplexing (TDM) and wave division multiplexing. For the future economical MFH, the TDM-PON is the preferable option, due to its simplicity and sharing of communications equipment (Zhou et al., 2018; Anthapadmanabhan et al., 2015).

A TDM-PON connects an optical line terminal (OLT), located at the CO, to a number of optical network units (ONUs) located on the customer's premises via a trunk fiber, an optical splitter, and a distribution fiber (International Telecommunication Union, G.984.5, 2014; International

Telecommunication Union, G.987.3, 2014). Figure 2 shows how it employs two wavelengths for transmission, one for traffic from OLT to ONUs (downstream), and another for traffic from ONUs to OLT (upstream). For the downstream direction, the OLT broadcasts to ONUs via the long trunk fiber with a passive power splitter that connects the ONUs through the distribution fiber (point-to-multipoint). For the upstream direction (multipoint-to-point), a number of ONUs have to share the trunk fiber towards the OLT, which requires some form of arbitration scheme. Since the OLT processes the centralized intelligence of the network, it bears the burden of this task. There are a number of studies presented in the literature dealing with the upstream dynamic bandwidth allocation (DBA) schemes for the TDM-PON, especially within the context of MFH (Kobayashi et al., 2016; Tashiro et al., 2014). Those DBAs are generally centralized at the OLT (co-located with the BBUs), which is located far away from the ONUs/RRHs. Such a DBA necessitates the exchange of control messages between the ONU and the OLT; this process suffers from a long roundtrip time (RTT) and consumes much-needed network bandwidth (in both directions) and OLT processing time. Consequently, it hinders overall network performance, specifically in the downstream direction.

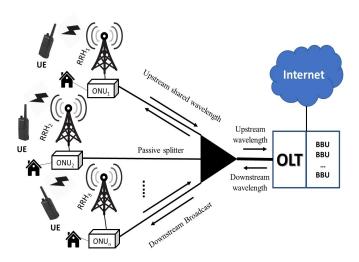


Figure 2. PON-supported 5G mobile fronthaul.

To overcome such a hindrance, the authors of this current study present a DBA that shifts the task towards the ONUs/RRHs from the distant OLT; that is, it relieves the OLT from the burden of continuous exchanges of control messages, which translates into added PON resources (in addition to eliminating the upstream RTT). The result was an enhanced downstream performance that offered lower latency, smaller queue sizes, and reduced packet loss.

TDM-PON Downstream Operation

The OLT houses N queues, where each queue corresponds to an ONU. The arriving traffic into the OLT is first

sorted according to the destination ONU addresses and then admitted into the corresponding queues (see Figure 3). The OLT polls the downstream queues cyclically to assess the transmission need; subsequently, it divides available downstream bandwidth among the queues and allocates transmission timeslots in which frames are broadcast downstream. Upon reception of the broadcasted frame, an ONU accepts the frame after matching the ONU's medium access control (MAC) address to the received frame's destination MAC address.

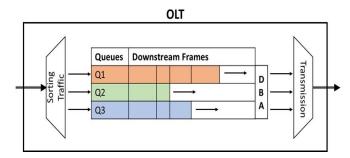


Figure 3. OLT's downstream configuration.

In a typical centralized TDM-PON architecture, the OLT bears the burden of performing the additional function of arbitrating shared upstream bandwidth among the ONUs, which impacts downstream operation. To implement such a scheme requires exchange of control messages between the OLT and ONUs; namely, REPORT (request) and GATE (grant) messages. These control messages are guided by the multi-point control protocol, as defined by the IEEE 802.3ah task force (IEEE, 2012). An ONU sends a RE-PORT message to the OLT requesting transmission bandwidth. The OLT uses the received REPORT to perform the bandwidth allocation computation. Then the OLT sends a GATE message to the ONU granting a transmission time slot (indicating the start time and the duration) in which the ONU transmits upstream traffic. Each ONU follows this process sequentially, requiring a short guard time between two successive transmissions. A cycle ends after every ONU completes the above process once (Kramer, Mukherjee, & Pesavento (2002). The cyclic OLT upstream task consumes network resources that impact downstream PON performance.

One of the elements that influences the downstream cyclic overhead is the upstream cycle length. The upstream cycle length varies in order to accommodate a variable traffic load; however, it is also restricted by a certain minimum and maximum duration. The cycle length can reach the maximum limit at a higher upstream load that should not exceed an MFH latency requirement of about 300 µs (Yoshimoto, 2014). On the other hand, the cycle length gets shorter in lower upstream loads. However, the minimum cycle length cannot be shorter than the RTT between an ONU and OLT, as the cycle length is the time between two consecutive GATEs to a specific ONU, which is equivalent to at least

one RTT (between the OLT and the ONU) (IEEE, 2012; Kramer et al., 2002). The RTT between the OLT and the ONU depends on the distance between them (e.g., RTT \sim 100 μ s and 200 μ s for \sim 10km and 20km trunk, respectively). The variable upstream cycle length is defined by Equation 1:

$$T_{upstream_cycle_min} = MAX \begin{cases} T_{rtt} \\ N \left(T_{guard} + (R/R_{PON}) \right) \end{cases}$$
 (1)

 $R_{PON} = ONU$ to OLT transmission line rates

R = ONU report size N = number of ONUs

 T_{guard} = guard time between two ONU upstream

transmissions

 T_{rtt} = round trip time between ONU and OLT

As the upstream cycle length gets shorter with decreasing loads, the number of upstream cycles per second rises significantly. This results in an increased transmission of GATEs, which translates to a heavier OLT task load and reduced available downstream bandwidth. Note that this hinders upstream performance as well, which is beyond the scope of this work (Hossain, Ummy, & Hossain, 2017). The downstream bandwidth loss due to upstream tasks can be estimated using Equation 2:

$$B_{downstream_loss}^{GATE} = \frac{1}{T_{unstream_cycle_min}} (N * G)$$
 (2)

where,

G = GRANT size in bits

 $T_{upstream_cycle_min}$ = minimum duration of upstream cycle N = number of ONUs

To illustrate this point, consider a network of 32 ONUs with a 10 km trunk length; such a network can suffer from a downstream overhead of 215 Mbps. Therefore, to address this issue, it is important to explore an alternative upstream resource allocation scheme.

MFH Upstream Distributed DBA

RRHs afford interconnectivity among themselves (via a simple interface such as X2 of LTE), which can be utilized by an ONU (connected to an RRH) to exchange its control information with other ONUs to support a fully distributed control plane for TDM-PON. Exploiting this advantage, the proposed scheme utilizes the wireless (RRH) network for the control tasks and the PON for transporting data traffic. In simpler terms, the upstream bandwidth allocation is now executed solely in the wireless plane (ONUs communicating with each other via the RRH), thus freeing up resources in the optical plane that would have otherwise been consumed by the control tasks.

Once the ONUs (via RRHs) exchange their control/report messages among themselves concerning their upstream transmission needs, each ONU concurrently and independently executes a common bandwidth allocation algorithm. Since all the ONUs receive identical network information and execute the exact same algorithm, they generate identical bandwidth allocation outcomes for the upstream PON cycle (data). Subsequently, the ONUs transmit their upstream traffic in a sequential manner, relieving the OLT from its centralized task of upstream DBA. Note that such a distributed approach primarily improves upstream performance (Hossain, Ummy, Hussain, & Kouar, 2017; Hossain, Dorsinville, Shami, Assi, & Ali, 2006). Additionally, it results in unhindered operation in the downstream direction. It is important to note that the proposed scheme only modifies the PON/MFH upstream DBA, while the rest of the C-RAN function remains centralized, as usual.

RRH Reporting

Figure 4 depicts the overall reporting process, while Figure 5 shows the corresponding flow diagram. Upon discovery of the neighboring RRHs, each RRH maps the network topology. Each ONU is connected to an RRH (collectively referred to as a node) through which it communicates wirelessly with other ONUs. The nodes cyclically exchange their current queue statuses among themselves via REPORT messages, which allows them to maintain a database of network information of all the nodes. The wireless report cycle starts concurrently from both end nodes of the network. Both end nodes, Node₁ and Node_n, concurrently transmit towards the center node, Node_c, where $c = [\{(n-1)/2\} + 1]$). Note that an odd number of nodes is considered for simplicity; however, for an even node count, there would be two center nodes (n/2 and n/2+1).

Reporting is implemented as follows:

- 1. Report Collection Stage
 - (a) Node₁ (from end node Node₁ towards the center node Node_c):

 In the forward direction, the first node (Node₂)
 - In the forward direction, the first node (Node₁) forwards its REPORT packet to the next (second) node (Node₂), which appends its own REPORT to the first node's REPORT and forwards it to the following (third) node (Node₃); this process continues until the aggregated REPORT packet reaches the center node (Node_c).
 - (b) Node_n (from end node Node_n towards the center node Node_c):
 - Simultaneously, the last node (Node_n) forwards its REPORT packet to the next (second last) node (Node_{n-1}), which appends its own REPORT and forwards it to the following (third last) node (Node_{n-2}); this process continues until the aggregated REPORT packet reaches the center node (Node_c).

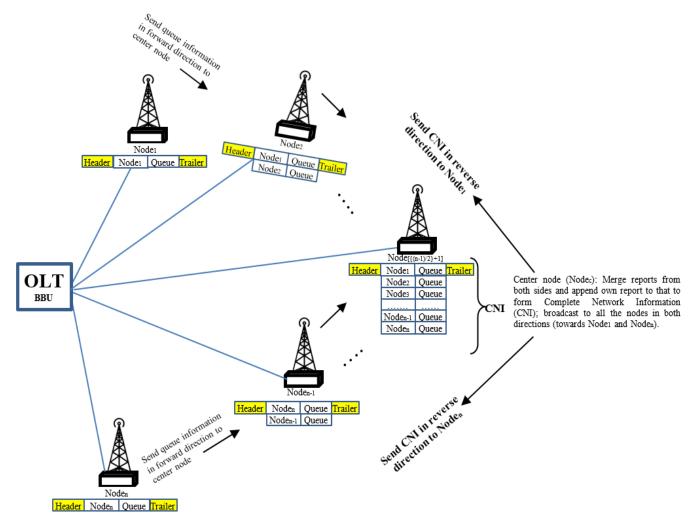


Figure 4. Overview of the distributed reporting scheme.

- Merge Reports (at center node Node_c)
 Once the aggregated reports reach the center node
 from both ends of the network, they are merged to gether with the center node's own REPORT into a
 single packet, which forms the complete network
 information (CNI).
- 3. CNI Distribution Stage (from center node Node_c toward the end nodes Node₁ and Node_n)

 In the reverse direction towards the end nodes, the CNI from the center node needs to be shared with all the other nodes in the network. This is accomplished by reversing the direction of the transmission described in #1. It flows concurrently from Node_c towards Node₁ and Node_n; thus, one flow is from Node_c to Node_{c+1} until Node₁. Note that there is no appending of information by each node as it forwards the CNI to the next node.
- 4. Execution of DBA Algorithm (all nodes)
 Once the CNI is received by all the nodes, each node executes an identical algorithm using the CNI, which results in timeslot assignments for each node for the next upstream PON cycle. The algorithm execution time is insignificant.

Once the algorithm is executed, the nodes sequentially transmit data traffic via the PON without any collisions; thus, eliminating the OLT's centralized task of DBA. Hence, this distributed scheme can support typical upstream resource allocation and other control tasks without resorting to the distant OLT. Therefore, unlike the typical centralized scheme, the entire downstream resource is available for the downstream network. As the downstream bandwidth and OLT resources are now fully dedicated to downstream traffic, any downstream allocation scheme should reflect improved performance. As such, a simple algorithm is able to take advantage of the distributed upstream DBA. It is im-

portant to address the issue of network reliability (protection and restoration), because there can be one or more failures in any part of the network, such as at the ONU, RRH, fiber, OLT, etc. While a detailed discussion of network reliability is beyond the scope of this paper, though is planned for a future study, the authors do offer a brief discussion. If there is a failure at the "RRH report collection stage" (e.g., an RRH fails - RRH_k), then the next RRH (RRH_{k+1}) in the forward direction waits until timeout, based on the expected arrival time as per start of the reporting cycle and propagation delays; once the waiting period ends, RRH_{k+1} transmits a "Network Failure" error message rather than a REPORT towards the forward direction. Each subsequent RRH merely repeats the error message without adding any report until it reaches the center RRH. At the center RRH, any report is ignored and the error message from RRH_{k+1} (indicating RRH_k failure) is copied to the CNI to broadcast in the reverse direction to all the RRHs; the network enters the "Failure Detection" phase and stops normal operation, due to this CNI (containing error message).

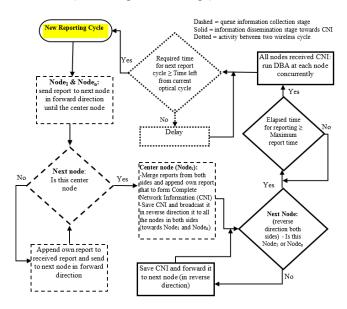


Figure 5. Flowchart of the distributed reporting scheme.

Due to the failure of RRH_k, the CNI does not reach any node from RRH_{k-1} to RRH₁ in the reverse direction. Consequently, utilizing the timeout mechanism (as above), those RRHs (RRH_{k-1} to RRH₁) conclude that there is a failure at some point prior to them and do not transmit anymore until a control message comes from the OLT to the attached ONUs. At this stage, the entire group of RRHs are aware of the network problem, some (RRH_{k+1} to RRH_n) via the CNI, while others (RRH_{k-1} to RRH₁) due to not receiving the CNI. As per normal scenario, upon bandwidth calculation, ONUs sequentially transmit (ONU₁ to ONU_n) in the upstream direction. Once the failure is detected, ONU_{k+1} is the first node that can transmit upstream traffic to the OLT at the beginning of next upstream optical cycle. Once the OLT

receives the error message, it broadcasts "Failure Recovery" instructions to the entire network; thus, the network enters the "Failure Recovery" phase. Details of this process will be addressed in a future study.

Downstream Allocation

As the OLT receives incoming traffic, it is sorted as per destination ONU addresses prior to admission into the queues. In each cycle, the OLT polls the downstream queues to assess the transmission need; subsequently, it divides available downstream bandwidth among the queues and allocates transmission timeslots. The downstream bandwidth is distributed among the queues, according to Equation 3:

$$B_{i}^{Granted} = \begin{cases} Q_{i} & \text{if } Q_{i} \leq B_{\text{max}} \\ B_{\text{max}} & \text{if } Q_{i} > B_{\text{max}} \end{cases}$$
 (3)

where.

$$B_{\text{max}} = \frac{1}{N} \Big[R_{PON} * T_{downstream_cycle_max} \Big]$$

 R_{PON} = downstream transmission rate

N = number of queues (downstream) in OLT

 $T_{downstream\ cycle\ max} = \max_{maximum\ cycle\ time}$

Q_i = downstream queue corresponding to ONU_i/RRH_i

In this case, a queue is granted bandwidth up to a predetermined maximum amount, B_{max} . When a queue request exceeds the maximum limit (B_{max}), it is granted additional bandwidth in the following cycle. This simple algorithm is called the fixed maximum limit.

Simulation and Results

The downstream simulation results are presented in this section to compare the centralized scheme with the distributed one. Two event-driven packet-based simulation programs (centralized and distributed) with identical network parameters were developed using C++. The performance metrics used here are average queuing delay, average queue occupancy, and packet loss ratio (PLR). For the sake of performance comparison between the two schemes, the following network parameters were used: an OLT with 16 queues (mapped to 16 ONUs/RRHs), a downstream transmission speed of 10 Gbps, a traffic arrival rate at each OLT queue of 1 Gbps, individual queue capacities of 100 MB, a trunk length of ~10 km, and a maximum downstream cycle time of 300 µs. These parameters were set arbitrarily, though any reasonable parameters would demonstrate the intended goals of the simulation.

To simulate as close as possible to a real-world scenario, the incoming downstream traffic was assumed to be uneven and bursty (Hossain et al., 2017). In other words, for a given average downstream network load, half of the queues had a higher network load, while the other half had a lower network load. The MFH packets arriving at the queue were assumed to be 1470 bytes (Mikaeil, Hu, Tong, & Hussain, 2017). Additionally, there were specific parameters associated with the centralized scheme, such as an upstream transmission rate of 10 Gbps, an upstream transmission guard time between two successive ONUs of 1 µs, an OLT downstream GATE message size of 84 bytes, and a processing time is 0.5 µs.

The downstream packets for OLT queues were generated with arrival times. As per arrival time, a packet was admitted in a first-in-first-out queue. At the scheduled transmission time of a specific packet, it was deleted from the queue. The queuing delay was defined as the time difference between the arrival and departure of the packet from a queue. Each point on the following figures is an averaged sample (40 million packets) of three different runs. Each figure is plotted in reference to the downstream total network load (TNL), which is the ratio of the average downstream load and the downstream link speed.

Figures 6 and 7 show the average downstream packet queuing delay and queue occupancy for the centralized and distributed schemes. The centralized delay was always longer than the distributed one (increasing from microseconds to milliseconds). Such a performance difference was attributed to less average bandwidth in the centralized scheme. At low downstream TNL, the available bandwidth was more than adequate to serve all the queues. However, the OLT's additional GATE function in the centralized scheme elongates the downstream cycle; consequently, the packets stay in the buffer longer (longer queuing delay). This is reflected in Figure 7, where a larger queue occupancy was consistent with a longer queueing delay for the centralized scheme. At a higher TNL, both schemes struggled to keep up with the network load, which resulted in a higher queuing delay. However, the distributed scheme still demonstrated better performance than the centralized scheme. At 78% TNL, the distributed scheme's queuing delay was ~200 µs, whereas the centralized scheme's queuing delay was ~400 µs. The centralized scheme exceeded the MHF delay requirement of 300 µs.

Figure 8 shows the PLR as a function of the TNL. The packet drop started when the queue became full. Figure 7 shows how the queue occupancy increased along with the network load; the queue reached maximum occupancy between 90% and 100% TNL. In a bursty traffic environment, both schemes showed packet drop at ~90% TNL. As seen previously, the queue occupancy grew much faster for the centralized scheme than the distributed one, resulting in higher packet drops for the centralized scheme. The packet drop was much more pronounced at ~100% TNL, when the centralized scheme showed a PLR of 4%, whereas the distributed scheme showed a PLR of 0.4%. The distributed scheme outperformed the centralized one.

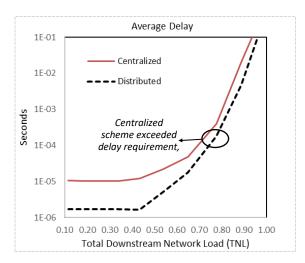


Figure 6. Average queuing delay for both schemes.

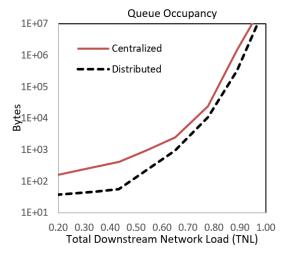


Figure 7. Average queue occupancy for both schemes.

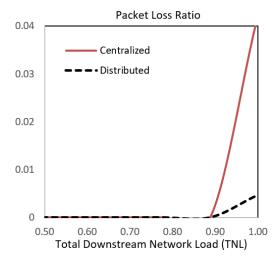


Figure 8. Average packet loss ratio for both schemes.

Conclusions

This study exploited the wireless connectivity in TDM-PON-based 5G MFH to exchange network information in order to support a fully distributed control plane, where the OLT was relieved from upstream resource allocation tasks. Specifically, the proposed distributed scheme, which exploited the wireless exchange of bandwidth information between the nodes via the RRH to alleviate the burden from the optical plane (by excluding the OLT from bandwidth allocation decisions for upstream traffic), resulted in significantly lower latency, smaller queue sizes, and reduced packet loss at all traffic loads. Potential future recommended areas of study can include a quality-of-service analysis of various traffic types and network protection and restoration in the event of various failures for both the optical and wireless planes.

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Multiscale Modeling of Aluminum Nickel-Coated Carbon Fiber Metal Matrix Composites

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Abstract

In this paper, the authors present a multiscale computational analysis of nickel-coated carbon fiber-reinforced aluminum metal matrix composite. The methodology involved different scale lengths ranging from nano to macro scales. In this hierarchical multiscale modeling technique, the outputs of each lower scale were fed into the next higher scale as input data. Molecular dynamics (MD) modeling was performed at the nano and micro scales, and polycrystalline materials modeling was done at the meso scale. A micromechanical model was utilized at the macro-length scale, and the results from these simulations provided the relationship between the microstructures of the constituents and the composite performance. The computational model provided the opportunity to quickly assess the ratios of the constituents in terms of volume fraction in the aluminum matrix composite products that are required for specific engineering performance.

Introduction

The need for the development of new materials to provide solutions to present day challenges of using traditional materials for different applications is increasing, due to the engineering requirements from high technology. In the quest for high-performance and lightweight structural materials for automotive and aerospace applications, researchers have innovated different material systems made up of more than one constituent. Metal matrix composite (MMC) is one of such material system from which engineers have combined different constituent materials to form a new product to overcome the limitations of each individual constituent. As such, the use of composite materials for engineering applications provides the flexibility for engineers to vary the ratio of the materials that constitute the composite in order to meet different requirements and performance standards. Hence, this current research study focused on aluminum matrix composites, due to their lightweight and outstanding specific properties at room or elevated temperatures (Lee, Sue, & Lin, 2010), which render them usable in the automobile and aerospace industries (Sozhamannan, Prabu, & Venkatagalapathy, 2012).

Other researchers (Kumar, Chittappa, & Vannan, 2018; Sharma, Khanduja, & Sharma, 2014; Surappa, 2003) have performed research studies on the mechanical performance

of aluminum matrix composites. According to Abraham, Pai, Satyanarayana, & Vaidyan (1992), aluminum (Al) and carbon do undergo a chemical reaction at the interface to form brittle aluminum carbide (Al₄C₃). Gupta, Nguyen, and Rohatgi (2011) performed a cooling analysis through nickel-coated carbon fibers in the solidification processing of aluminum matrix composites and found that thermal stresses can cause failure of the nickel coating. Hua et al. (2012) performed electroplating technique to test coat carbon fibers with nickel. Their results indicated that nickel-coated fibers exhibited good bonding strength, the wettability of aluminum was improved, and the fibers exhibited excellent resistance to oxidation at high temperatures.

A concerted effort was made (Kumar, Rao, & Selvaraj, 2011) to strengthen some mechanical and wear behavior of Al—MMCs, and the prediction of the mechanical and tribological behaviors of aluminum MMCs. High-resolution electron microscopy and X-ray photoelectron spectroscopy were utilized (Diwanji & Hall, 1992) to analyze the carbon/aluminum matrix interface, and showed that carbide formation is a conventional two-step process of nucleation and growth. Other authors (Lacin & Marhic, 2000) used a transmission electron microscope to fully characterize the microstructure of the high modulus PAN-based fiber and the pyrolytic carbon coating (Cp). Nickel-coated carbon fibers were mixed, consolidated, and heated with AA6061 aluminum powders at temperatures ranging from 650°C to 950°C, in order to study the reactivity, the nickel (Ni) diffusion, and the resulting interfaces. Alfos et al. (2015) evaluated the effects of Young's modulus on Al₄C₃ formation in the carbon nanotube (CNT)-Al interface for Al matri composites using finite element analysis (FEA) models that incorporate different CNT volume fractions and interfacial Al₄C₃ layers of various thicknesses.

Similarly, Choi, Yoon, and Lee (2016) investigated the mechanical behavior of CNT-reinforced aluminum composite under a tensil loading condition using molecular dynamic (MD) simulations. In addition, Nasiri, Wang, Yang, Li, and Zaiser (2019) utilized a multiscale approach to analyze nickel-coated carbon nanotubes in aluminum matrix composites. With the increased emphasis on reducing the cost and time to market of new materials, the need for multiscale analysis to capture the effect of the nanostructured additive on the composite matrix is increasingly important. This multiscale modeling approach revolutionizes the ability to create new materials and tailor their specific

properties. In spite of the extensive research work that has been done on aluminum matrix composites, little or no work has been done on multiscale approaches that link material models at multiple time and length scales. For example, it is important to link manufacturing processes, which produce internal material structures that in turn influence material properties and which can be engineered at the macroscopic scale to meet specific product requirements and performances. In addition, there is no established link between mechanical properties of composites, volume fraction, and type of reinforcement.

The focus of this current investigation was to establish a multiscale framework that could provide a correlation between the molecular structure of the material phases, the arrangement of the phases in the constituents, the volume fraction of the constituents, and the morphology of the constituents in the composite in terms of the mechanical performance of the composite material. To measure the properties at such a small length scale can be difficult and costly. Furthermore, experimental data at this scale may contain some unknown errors; as such, computational simulation results can be used to validate experimental data and conclusions. Thus, multiscale analysis requires the establishment and validation of MD simulations to evaluate the mechanical properties of the different material phases in an aluminum matrix composite. In this study, MD models of Al, carbon fiber (C_f), and crystalline Ni were generated using a largescale atomic/molecular massively parallel simulator (LAMMPS) in order to predict their elastic properties at the nano-length scale. The results from these MD models were used as inputs for obtaining their polycrystalline properties, which were in turn used as input data for continuum-level prediction using the generalized method of cells (GMC) micromechanics theory to evaluate the mechanical properties of the composite.

Molecular Dynamics Modeling of Crystalline Aluminum, Carbon Fiber, and Nickel

In the application of molecular modeling methods to the nanoscale analysis of structures, carbon fiber is often approximated as graphene to reduce the number of atoms needed to fully represent the fiber. Figure 1 shows the monolayer graphene that was built using the LAMMPS package with Tersoff (1989) potential and periodic boundary conditions. The primitive vectors, given in Equation 1, for graphene structure were used to construct the primitive cell that was replicated in the x- and y-directions to create a supercell crystalline model.

$$a_1 = ai$$
 (1a)

$$a_2 = 0.5ai + \frac{\sqrt{3}}{2}aj$$
 (1b)

$$a_3 = ak \tag{1c}$$

where, a = 2.46 Å

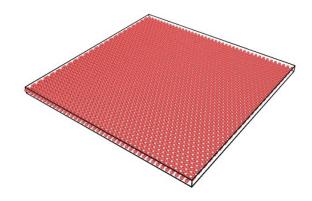


Figure 1. Size of graphene supercell ($103.32 \times 103.32 \times 3.6$ with 16,128 atoms).

The aluminum and nickel were constructed using Zope-Ti-Al-2003-eamalloy (Zope & Mishin, 2003) and FeNiCr.eam.alloy (Bonny, Terentyev, Pasianot, Ponce, & Bakaev, 2011) potentials, respectively, with primitive vectors given by Equation 2:

$$a_1 = \frac{1}{2}a(j+k) \tag{2a}$$

$$a_2 = \frac{1}{2}a(i+k) \tag{2b}$$

$$a_3 = \frac{1}{2}a(i+j) \tag{2c}$$

where, a = 4.05Å for aluminum, and a = 3.52Å for nickel.

Figures 2 and 3 show the supercells for the Al and Ni structures, respectively. All of the structures created were relaxed by performing MD simulations using the NVT (constant number of atoms, volume, and temperature) ensemble at 300K for a period of 100 ps. To further reduce the internal forces and residual stresses that were created from the initial construction of the bonds and the bond angles, minimization was performed over 100 ps at a temperature of 300K using the conjugate gradient stopping criterion. Upon completion of the initial relaxation process, the final equilibration of the systems was carried out under the NPT ensemble at 300K for 1000 ps using a time step of 0.08 fs and Nose-Hoover barostat and thermostat.

Evaluating the Elastic Properties from MD

In order to obtain the required stress-strain relationship for evaluating the elastic constants, the equilibrated structures were mechanically deformed. A distinct displacement vector was imposed to determine each elastic constant. The "fix deform" command in LAMMPS was utilized to determine c₁₁ and c₁₂, with an axial strain applied in the x-direction on the periodic models under the NVT ensemble at a temperature of 300K and one atmosphere. The corresponding stress components were evaluated independently for a complete stress-strain response. NVT simulations were run for 1000 ps with time steps of 0.08 fs. The deformation was done at an engineering strain rate of 10⁻⁵/ps using the erate command in order to obtain a desired strain magnitude of 0.01 in the x-direction, while strains along the y- and z-axes were kept at zero. The overall elastic constant of the model (in the loading direction) was obtained from the plot of the stress-strain curve using each time step.

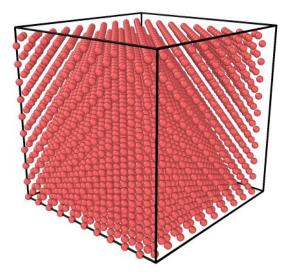


Figure 2. Size of Al supercell (80.9 x 80.9 x 80.9 with 32,000 atoms).

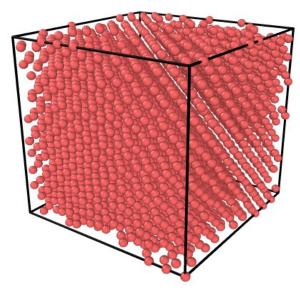


Figure 3. Size of Ni supercell $(70.4 \times 70.4 \times 70.4 \times 32,000)$ atoms).

The virial stress $\sigma_{\lambda\gamma}$ (Zhao & Xue, 2013; Subramaniyan & Sun, 2008) computed from Equation 3 was utilized to obtain the stress-strain curve during tensile loading.

$$\sigma_{\lambda\gamma} = \frac{1}{V} \left(\sum_{i=1}^{N} m v_{\lambda}^{i} v_{\gamma}^{i} + \frac{1}{2} \sum_{i=1}^{N-1} \sum_{j=i+1}^{N} r_{ij,\lambda}^{N-1} F_{ij,\gamma} \right) (3)$$

where, V is the entire volume of the material in the simulation cell; λ and γ are the indices in the Cartesian coordinate system; m and V^i_{λ} indicate the mass and λ -component velocity of atom i; and, $r_{ij,\lambda}$ and $F_{ij,\gamma}$ indicate the λ -component of the separation and the γ -component of the force between atoms i and j, respectively.

To obtain the corresponding elastic constant, a linear regression analysis was performed on the obtained data. It is worth noting that the above virial stress was the true stress. However, engineering stress (σ) and strain (ϵ) were obtained using Equations 4 and 5, respectively:

$$\sigma = \frac{\sigma_{\lambda \gamma}}{(1 + \varepsilon)} \tag{4}$$

$$\varepsilon = \frac{L - L_O}{L_O} \tag{5}$$

where, L and L_o are the current and original lengths in the loading direction, respectively.

It is important to note that the engineering stress obtained from Equation 4 is related to the stress obtained from strain energy density U, given by Equation 6 (Rassoulinejad-Mousavi, Mao, & Zhang, 2016):

$$\sigma_{ij} = \frac{\partial U}{\partial e_{ii}} \tag{6}$$

The stress components are given by Equation 7:

$$\sigma_{xx} = C_{11}e_{xx} + C_{12}\left(e_{yy} + e_{zz}\right) \tag{7a}$$

$$\sigma_{yy} = C_{11}e_{yy} + C_{12}\left(e_{xx} + e_{zz}\right) \tag{7b}$$

$$\sigma_{zz} = C_{11}e_{zz} + C_{12}(e_{xx} + e_{yy})$$
 (7c)

$$\tau_{xy} = C_{44} e_{xy} \tag{7d}$$

Also, a planar shear strain was applied incrementally to each MD model. The corresponding shear stress, τ_{xy} , was evaluated for each time step. It is important to note that this simulation was performed under the NVT ensemble at 300K, and atmospheric pressure at a constant engineering shear strain rate of 10^{-5} /ps using the erate command. A linear regression analysis was performed in order to obtain the simulated stress-strain data that were utilized to determine the elastic constants, c_{44} .

The MD Results

The micro constituents of aluminum metal matrix composite structures—consisting of graphene, nickel, and aluminum—were created in LAMMPS. Tables 1-3 shows comparisons of the average value of the elastic constants obtained from the three independent models of each constituent to available data from the literature. The predictions were in relative agreement with these data and serve as validation for the MD methods used. Furthermore, as monolayer graphene is a 2D isotropic sheet, the linear elastic constants should satisfy the condition $2C_{44} = C_{11} - C_{12}$, as can be verified from Table 3.

Table 1. Average elastic stiffness constant of Aluminum in comparison with experimental data (Vallin, Mongy, Salama, & Beckman, 1964).

Property	Present MD	Expt.
C ₁₁ (GPa)	98.31	107.30
C ₁₂ (GPa)	53.68	60.08
C ₄₄ (GPa)	26.36	28.3

Table 2. Average elastic stiffness constant of nickel in comparison with experimental data (Ledbetter & Reed, 1973).

Property	Present MD	Expt.
C ₁₁ (GPa)	247.24	253.00
C ₁₂ (GPa)	135.98	152.00
C ₄₄ (GPa)	112.58	124.00

Table 3. Average elastic stiffness constant of GNP in comparison with analytic data (Thomas, Ajith, Lee, & Valsakumar, 2018).

Property	Present MD	Analytic
C ₁₁ (GPa)	933.843	989
C ₁₂ (GPa)	270.000	221
C ₄₄ (GPa)	330.000	380

The Effective Elastic Behavior of a Polycrystalline Material

The elastic constant obtained from the MD simulation represents the result for a single crystal, which is an approximate solution for the polycrystalline material. A single crystal will generally not be isotropic, but the degree of symmetry of the crystal structure controls the number of the material constant. There are three parameters (c_{11} , c_{12} , and c₄₄) for cubic structures (Nye, 1985). It has been shown that isotropic materials also have three elastic constants (den Toonder, van Dommelen, & Baaijens, 1999). Even though all grains will generally be anisotropic in their behavior, in which they depend on their crystal structure and orientation at the microscopic scale, when the number of grains are sufficiently large and they are randomly orientated, the effective macroscopic behavior will be isotropic. Therefore, their constitutive properties can be characterized by Young's modulus and Poisson's ratio. The effective macroscopic material properties are determined by averaging the anisotropic elastic properties of the individual grain over all possible grain orientations (den Toonder et al., 1999). Voigt's averaging scheme is based on the assumption that the strains are continuous, while the stresses are allowed to be discontinuous. For this reason, the forces between grains will not be at equilibrium and this method will give upper bounds for the actual effective constants defined by Equations 8 and 9:

$$B_V = (c_{11} + 2c_{12})/3 (8)$$

$$G_V = (c_{11} - c_{12} + 3c_{44})/5 \tag{9}$$

The Reuss averaging method assumes that the strains are discontinuous and stresses are continuous. As a result, the deformed crystals will not fit together and the lower bound effective properties are obtained. The Reuss effective constants are computed from Equations 10 and 11:

$$B_{R} = (c_{11} + 2c_{12})/3 \tag{10}$$

$$G_R = 5c_{44} \left(c_{11} - c_{12} \right) / \left(4c_{44} + 3\left(c_{11} - c_{12} \right) \right) \tag{11}$$

In this study, the Voigt-Reus-Hill method that combines the lower and upper bounds was applied by assuming the average of the Voigt and the Reuss elastic constant to be a better approximation for the actual macroscopic effective elastic constant. This average value can be determined from Equation 12:

$$G_{VRH} = (G_V + G_R)/2; \ B_{VRH} = B_V = B_R$$
 (12)

where, B and G are bulk and shear modulus, respectively.

Knowing B and G, the Young's modulus and Poisson's ratio can be determined from the isotropic relations given by Equations 13 and 14:

$$E = 9GB/(3B+G) \tag{13}$$

$$v = (3B - 2G)/2(3B + G)$$
 (14)

Table 4 gives the current predictions for the macroscopic effective elastic constants.

Table 4. Properties of graphene, nickel, and aluminum.

Property	Aluminum	Nickel	Graphene
E (GPa)	71.1290	218.7700	810.422
ν	0.4423	0.2893	0.2251
G (GPa)	24.6570	84.8400	330.767

Micromechanical Model for Three-Phase Al/C_f/Ni Composites

Micromechanical analysis of the heterogeneous materials is the next higher length scale analysis required for determining the effective properties of the composite; the input data are the results obtained from the analysis of polycrystalline theory. In this study, continuum-level predictions using GMC micromechanics theory was performed (Paley & Aboudi, 1992; Bednarcyk, Aboudi, & Arnold, 2014; Aboudi, Arnold, & Bednarcyk, 2013; Bednarcyk & Arnold, 2002). The GMC for continuous or discontinuous fibrous composites make effective use of a repeating unit cell (RUC) that represents the periodic material microstructure. This may comprise some arbitrary phases required to correctly model the composite material. For this reason, the GMC has the ability to model any arbitrary multiphase composite. The basic methodology utilized for homogenization in micromechanics is made up of four steps (Bednarcyk & Arnold, 2002). First, identify the repeating volume element (RVE) of the periodic composite. Second, define the macroscopic or average stress and strain state in terms of the individual microscopic sub-cell. Third, impose the continuity of tractions and displacements at the boundaries between the constituents. Then, combine these three steps with microequilibrium to establish the relationship between micro (sub -cell) total, and macro (composite) strains via the relevant concentration tensors. In this step, the overall macro constitutive equations of the composite are obtained. These four steps form the basis of the micro-to-macro-mechanics analysis, which describes the behavior of heterogeneous materi-

The result of the micromechanical analysis defines the overall (macro) characteristics of the multi-phase composite and is communicated as a constitutive relationship between the average stress and strain, linked by the effective elastic stiffness. The implementation of GMC is enhanced by the MAC/GMC software package, developed by the NASA Glenn Research Center (Bednarcyk & Arnold, 2002). The micromechanical analysis of the composite was executed using software and the corresponding properties of the micro-constituents of composites in the MAC/GMC analysis to model the three-phase Al/Ni/carbon fiber composites. A detailed explanation of the steps are documented in the following sections. Figure 4 depicts the modeling techniques for using the molecular-scale properties to ultimately predict the elastic properties of MMC.

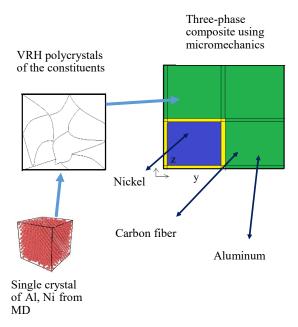


Figure 4. Multiscale modeling technique.

The properties of sub-cells representing the unit cell comprising carbon fiber (C_f), Ni, and Al matrix were taken from Table 4. The above formulation allows the elastic constants of the MMC composites to be easily computed for any arbitrary volume fraction of the constituents. It is important to note that MAC/GMC has the capability to use many different micromechanical analysis models and unit cell architectures for carbon fibers. Figure 5 shows how the analysis of continuous fibers, RUC 2x2 doubly periodic micromechanics model (MOD=2), and the fiber architecture ID (ARCHID =1) for three-phase MMC composites was chosen. This figure contains sub-cells of carbon fibers (blue), Ni as the interphase (yellow), and Al as the matrix phase (green) to simulate the three-phase Al/ C_f/Ni composite. In the analysis, a linear elastic constitutive model (CMOD=6) was used, loading was strain-controlled (MOD=1) with a strain magnitude of 2%, the fiber radii was 7 µm, and the ratio of interface thickness to fiber radius (RITFR) was 0.07.

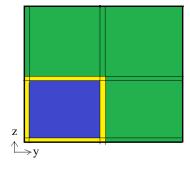


Figure 5. The RUC architecture (ARCHID=1), blue= $C_{\rm f}$, yellow-Ni, and green=Al.

Figure 6 shows how the analysis of short fibers, RUC triply periodic micromechanics model (MOD=3), and the fiber architecture ID (ARCHID =2) for the three-phase MMC composites was also chosen.

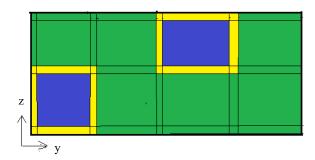


Figure 6. The RUC architecture (ARCHID=2), blue=C_f, yellow-Ni, and green=Al.

To establish the validity of the present methodology, the available experimental data of aluminum nickel-coated short carbon fiber metal matrix composites in the literature (Kumar et al., 2018) was utilized. In their experimental investigation, the authors used nickel-coated fibers with an average diameter of $7\mu m$ and a length of about 1.0-1.5 mm.

Results and Discussion

The three-phase MMC making up the Al structures, carbon fibers (C_f), and Ni were modeled using micromechanics theory. The elastic moduli, shear moduli, and Poisson's ratios for each model were obtained from macroscopic theory of polycrystalline materials. Tables 5 and 6 document the predicted effective properties of the three-phase Al/ C_f /Ni composites using MAC/GMC software for continuous and short fibers, respectively. Table 5 shows how the computational results of continuous fibers at different volume fractions of carbon fibers (V_f) can be used to optimize the performance of the MMC composites. The results generally showed that the structural properties of the MMCs depended on their microstructural constituents. It was clearly demonstrated that the composite was transversely isotropic with stiffness greater in the fiber direction.

Table 5 shows that the range of E_1 for the composites was 71.89-261.88 GPa, while that for E_2 was 71.35-137.16 GPa. The E_1 and E_2 data are also presented visually on the graph in Figure 7. However, the numerical results were normalized by 71.89 GPa for E_1 and 71.35 for E_2 in order to compare the two. Figure 7 shows that E linearly increases with increased carbon fibers in both longitudinal and transverse directions. Table 6 documents the effective properties of aluminum nickel-coated short carbon fiber metal matrix composites. As noted previously, the fiber's average diameter of 7 μ m and length of 1.2 mm were used to compare the results with the experimental data found in the literature (Kumar et al., 2018).

Table 5. The effective properties for the three-phase composites $Al/C_f/Ni$ for continuous fibers.

V_{f}	0.0	0.05	0.10	0.15	0.20	0.25
E ₁ (GPa)	71.89	109.25	147.40	185.57	223.73	261.88
E ₂ (GPa)	71.35	81.80	92.77	105.26	119.93	137.16
E ₃ (GPa)	71.35	81.80	92.77	105.27	119.93	137.16
G ₁₂ (GPa)	24.68	26.27	28.31	30.73	33.58	36.91
G ₁₃ (GPa)	24.68	26.27	28.31	30.73	33.58	36.91
G ₂₃ (GPa)	24.68	25.99	27.48	29.15	31.04	33.19
v_{12}	0.442	0.430	0.418	0.405	0.393	0.381
v_{13}	0.442	0.430	0.418	0.405	0.393	0.381
v_{23}	0.445	0.538	0.578	0.592	0.591	0.580

Table 6. The effective properties for the three-phase Al/C_f/Ni composites for short fibers.

$V_{\rm f}$	0.0	0.05	0.10	0.15	0.20	0.25
E ₁ (GPa)	71.13	75.78	81.32	87.35	93.70	100.26
E ₂ (GPa)	71.13	75.59	80.81	86.45	92.38	98.50
E ₃ (GPa)	71.13	75.59	80.81	86.45	92.38	98.50
G ₁₂ (GPa)	24.66	25.94	27.42	29.08	30.94	33.02
G ₁₃ (GPa)	24.67	25.94	27.42	29.08	30.94	33.02
G ₂₃ (GPa)	24.67	25.94	27.29	28.80	30.45	32.22
v_{12}	0.442	0.441	0.439	0.437	0.435	0.433
v_{13}	0.442	0.441	0.439	0.437	0.435	0.433
v_{23}	0.442	0.441	0.440	0.439	0.4378	0.4362

These data showed that the Young's modulus of aluminum nickel-coated carbon fiber metal matrix composite ranged from 73 to 90 GPa for a weight fraction in the range 0-0.08 (0-0.1231 vol. fraction) of carbon fiber. In this current study, a volume fraction of carbon fiber ranging from 0 to 0.25 (see again Table 6) was compared with experimental data results (see Table 7). The value of E was in agreement with the experimental data. However, the subtle difference between the two data might be due to the length

variation of the carbon fibers used in the experiment. While the present study utilized a fiber length of 1.2 mm, the fiber's lengths within the aluminum matrix were cut to about 1.0-1.5 mm. Tables 5 and 6 also show the effect of volume fraction of C_f on shear modulus G and Poisson's ratio ν . In both cases, while G increased with volume of carbon fibers, ν generally decreased with increases in C_f . It is important to note that further analysis beyond elastic properties, such as yielding behavior, failure strength, and toughness of these composites at room and elevated temperatures, are recommended for investigation.

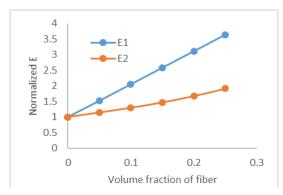


Figure 7. Young's modulus as a function of volume fraction for continuous fibers.

Table 7. Young's modulus (in GPa) of short fibers in comparison with experiment.

V_f of C_f	Present study	Expt. [Kumar et al.]
0.0000	71.129	73.000
0.0308	73.841	77.000
0.1231	84.056	90.000

Conclusions

The micromechanics analysis method was used to predict the mechanical properties of three-phase MMC using MAC/ GMC. The microstructures of the constituents in the Al matrix composites contained different phases—crystalline Al, carbon fiber, and Ni. Different volume fractions of carbon fibers were utilized in the analysis. The properties of the constituents were obtained from MD simulations and macroscopic theory of polycrystalline materials. The current predictions were in agreement with the available data in the literature and serve as validation for the MD, theory of polycrystalline materials, and micromechanics methods used. The predictions showed that the modeled properties of MMC composites heavily depend on the microstructural constituents of the composites and the volume fraction of constituent materials. As such, the model can be used to quickly assess the proportional ratio of the constituents in a MMC product that will be needed to meet particular performance requirements.

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